

**Injectable Resorbable Bone Graft Material, Powder for Forming Same and  
Methods Relating Thereto for Treating Bone Defects**

RELATED APPLICATIONS

This application claims priority to United States Provision Patent Application Serial Number 60/444,690, filed February 4, 2003.

BACKGROUND OF THE INVENTION

Field of the Invention:

(0001) The present invention pertains to bone graft materials and, more particularly, to resorbable bone graft materials optimized for strength, injection and osteoconductivity and to methods of strengthening bones using injectable, resorbable bone graft materials.

Brief Discussion of the Related Art

(0002) Minimally invasive surgical procedures have become very popular in the orthopedic field; and accordingly, it has become desirable to be able to inject bone graft materials in a minimally invasive manner, such as via a syringe. Since it is desirable for some bone graft materials set or cure in the body, time constraints are an issue in that the bone graft materials must maintain sufficiently low viscosity to allow injection without requiring substantial ejection force but, after injection, should, desirably, cure quickly to provide compression strength as soon as possible. Additionally, it is preferred that bone graft materials be resorbable (bioabsorbable), as opposed to bone cement which is not, and osteoconductive. The MIIG® 115 injectable bone graft material, described in US Published Patent Application 2003/0185903 and marketed by Wright Medical Technology, Inc., the assignee of the present invention, is an effective injectable resorbable bone graft material made from calcium sulfate hemihydrate; however, improvements are desirable relating to working time (the time period available in which the bone graft material can be implanted in the body), injectability (the relative force

required to easily inject the bone graft material through associated instrumentation using hand and/or thumb force), the set or cure time relative to compressive strength, the compressive strength achieved one hour after injection and the compressive strength achieved 24 hours after injection. Calcium sulfate hemihydrate for use as bone graft materials have, in the past, been made using hydrothermal processes where calcium sulfate dihydrate is boiled in a reaction vessel under greater than atmospheric pressure and result in a structure which requires an undesirable amount of water for hydration.

### SUMMARY OF THE INVENTION

**(0003)** The present invention provides a high strength, injectable resorbable bone graft material for treating bone defects by implanting or injecting the injectable resorbable bone graft material therein. The term "bone defects" as used herein includes, but is not limited to, defects or voids/gaps resulting from compression fractures, benign bone cysts, diseased bone, high energy trauma, peri-articular fractures, cranial-maxillo facial fractures, osteoporotic reinforcement (ie. screw augmentation), joint arthrodesis, joint arthroplasty and periodontal reconstruction.

**(0004)** The injectable resorbable bone graft material of the present invention is particularly useful for minimally invasive insertion in bone defects to provide a temporary support media as well as a resorbable graft, the bone graft material being osteoconductive and replaced by bone.

**(0005)** The injectable bone graft material according to the present invention permits injection up to 5 minutes after mixing of calcium sulfate hemihydrate powder, with or without an accelerant, with a diluent to produce a paste, the paste achieving, within 10 minutes after injection, a compressive strength of cancellous bone, within 20 minutes after injection, achieving a compressive strength of at least the upper end of cancellous bone, and, within 24 hours after injection, achieving a compressive strength well above cancellous bone.

### BRIEF DESCRIPTION OF THE DRAWINGS

(0006) Figure 1 is a scanning electron micrograph (SEM) depicting the crystalline structure of the calcium sulfate hemihydrate used in the present invention and in particular how it is formed of thick, stubby rod-like crystals prior to milling.

(0007) Figure 2 is a scanning electron micrograph (SEM) depicting the crystalline structure of the calcium sulfate hemihydrate used in the present invention and in particular how it is formed of thick, stubby rod-like crystals after milling.

### DESCRIPTION OF THE PREFERRED EMBODIMENT

(0008) In accordance with the present invention, a powder is provided composed of calcium sulfate hemihydrate, in a range from 99.8% to 100% and, if the calcium sulfate hemihydrate is less than 100%, an accelerant (or accelerator), preferably calcium sulfate dihydrate, up to 0.20% may be added. The powder, calcium sulfate hemihydrate or a blend including the accelerant, is mixed with a diluent, such as sterile water, prior to insertion (or implant) in bone, the diluent to powder weight ratio range being from 0.19:1 to 0.31:1. The calcium sulfate hemihydrate is made by a known process, as disclosed in US Patent 2,616,789, whose contents are incorporated entirely herein by reference, where calcium sulfate dihydrate is immersed in a solution of water and an inorganic salt, such as magnesium chloride, calcium chloride, sodium chloride or other biocompatible inorganic salts selected from ammonium chloride, ammonium bromide, ammonium iodide, ammonium nitrate, ammonium sulfate, calcium bromide, calcium iodide, calcium nitrate, magnesium bromide, magnesium iodide, magnesium nitrate, sodium bromide, sodium iodide, sodium nitrate, potassium chloride, potassium bromide, potassium iodide, potassium nitrate, caesium chloride, caesium nitrate, caesium sulfate, zinc chloride, zinc bromide, zinc iodide, zinc nitrate, zinc sulfate, cupric chloride, cupric bromide, cupric nitrate, cupric sulfate alone or together. The calcium sulfate dihydrate and the solution are heated to substantially the boiling point at atmospheric pressure

until a substantial portion of the calcium sulfate dihydrate is converted to calcium sulfate hemihydrate. The resulting calcium sulfate hemihydrate has a different crystalline structure than calcium sulfate hemihydrate produced by hydrothermal processes and has a lower water-carrying capacity after being milled (Figure 2) according to conventional methods as described in the patent, but for in vivo orthopedic applications. In particular, the crystalline structure of the calcium sulfate hemihydrate used in the present invention is formed of thick, stubby rod-like crystals, as disclosed in US Patent 2,616,789 (Figure 1).

**(0009)** Mixing of the powder with the diluent forms a paste that is intended to be injected into bone defects, as defined above, that are not intrinsic to the stability of bony structure of the skeletal system (i.e., the extremities, spine, and pelvis) and to cure in situ. The bone defects may be surgically created osseous defects or osseous defects created from traumatic injury to the bone. The paste provides a bone void filler that resorbs and is replaced with bone during the healing process. The injectable resorbable bone graft material paste cured in situ provides an open void/gap filler that augments provisional hardware (e.g., K-Wires) to help support bone fragments during surgical procedures. The cured paste acts only as a temporary support media and is not intended to provide structural support during the healing process. In use, needles are pre-placed in defects under fluoroscopic guidance. The plunger is removed from a syringe and set aside. The powder and sterile water are placed in a bowl and mixed, preferably in a vacuum mixer. Preferably, the calcium sulfate paste is mixed in one direction for 30 seconds at a vacuum of approximately 22-25mmHg. While mixing, the bowl should be tapped to keep the paste in the mixing zone. After mixing, a spatula is used to transfer the paste to the syringe. After the plunger is replaced, the syringe is inverted, and the plunger is advanced to remove air. The syringe is then docked to a pre-placed needle, and injection is initiated with steady thumb pressure. The total injection time should be approximately 2.5 minutes.

**(0010)** As noted above the calcium sulfate hemihydrate has low water-carrying capacity and is formed of thick, stubby rod-like crystals, as disclosed in US Patent 2,616,789. Such calcium sulfate hemihydrate has not been used, prior to the present invention, as a bone graft or substitute material. Unexpectedly, such calcium sulfate hemihydrate allows optimizing of action times and compressive strength as well as being resorbable, that is absorbable in the body within a time required to permit bone defect healing.

**(0011)** In accordance with the present invention, after mixing, a working time of 5 minutes or greater, depending on the amount of diluent or accelerant added, can be achieved to permit the injectable resorbable bone graft paste to be loaded into the syringe and to be injected into the bone, e.g. via the syringe and pre-placed needle. At the same time, the injectable resorbable bone graft material sets or cures quickly in the body to provide improved compressive strengths from prior art bone graft materials.

**(0012)** The accelerant is believed to enhance, e.g., accelerate, the conversion of calcium sulfate hemihydrate to calcium sulfate dihydrate. In particular, it is believed that particles of the accelerant act as crystallization nucleation sites for the conversion of calcium sulfate hemihydrate to calcium sulfate dihydrate. Examples of accelerants include calcium sulfate dihydrate, potassium sulfate and sodium sulfate. Other examples include ionic salts. A preferred accelerant is calcium sulfate dihydrate crystals (available from U.S. Gypsum) coated with sucrose (available from VWR Scientific Products). A process of stabilizing the dihydrate crystals by coating with sucrose is described in U.S. Patent No. 3,573,947, hereby incorporated by reference in its entirety. Mixtures of two or more accelerants can be used.

**(0013)** The diluent is generally selected to provide the composition with a desired consistency and hardening time. Examples of diluent include water, e.g., sterile water, solutions containing inorganic salts, or cationic surface active agents including sodium chloride, saline, e.g., phosphate buffered saline, potassium chloride, sodium sulfate,

potassium sulfate, EDTA, ammonium sulfate, ammonium acetate, and sodium acetate. Mixtures of two or more diluents can be used.

**(0014)** The diluent can further include, for example, bone marrow aspirate, platelet concentrate, blood, pharmaceutical additives in solution, or combinations of these materials. Examples of additives are medicaments or pesticides. Examples of medicaments are antibiotics, chemotherapeutic agents, growth factors, and analgesics. Examples of antibiotics are tetracycline hydrochloride, vancomycin, cephalosporins, and aminoglycosides such as tobramycin and gentamicin. Examples of chemotherapeutic agents are cis-platinum, ifosfamide, methotrexate, and doxorubicin hydrochloride (Adriamycin®). Examples of growth factors are transforming growth factors beta (TGF-Beta), bone morphogenic protein (BMP), basic fibroblast growth factor, platelet-derived growth factor, and other polypeptide growth factors. Examples of analgesics are anesthetics such as lidocaine hydrochloride (Xylocaine®), bupivacaine hydrochloride (Marcaine®), and non-steroidal anti-inflammatory drugs such as ketorolac tromethamine (Toradol®).

**(0015)** As will be appreciated from the foregoing, the present invention produces an injectable resorbable bone graft material for minimally invasive implant in a bone defect utilizing a powder comprising calcium sulfate hemihydrate mixable with a diluent in a diluent to powder weight ratio from 0.19:1 to 0.31:1 to form an injectable paste and utilizing a powder formed of calcium sulfate hemihydrate and an accelerant, and a diluent mixed with the powder, the calcium sulfate hemihydrate forming, by weight, from 99.8% to 100% of the powder, the accelerant forming, by weight, from 0% to 0.2% of the powder, and the diluent to powder weight ratio being from 0.19:1 to 0.31:1. In a specific example, the accelerant is calcium sulfate dihydrate and the diluent is sterile water, the calcium sulfate hemihydrate forms 99.99% of the powder by weight, the calcium sulfate dihydrate forms 0.01% of the powder by weight and the sterile water to powder weight ratio is 0.25:1. Additionally the present invention includes treating bone

defects by injecting a resorbable bone graft material in the form of a paste by mixing calcium sulfate hemihydrate having thick stubby rod-like crystals with water.

(0016) The following examples show the efficacy of the inventive materials and methods according to the invention.

#### Example One

(0017) A 35-gram mixture of powder having 99.995% calcium sulfate hemihydrate manufactured as described above and 0.005% calcium sulfate dihydrate is placed into a bowl with about 8.75g of water and the two are mixed (water-to-powder ratio =0.25), preferably in a vacuum mixer. Preferably the calcium sulfate paste is mixed in one direction for 30 seconds at a vacuum of approximately 22-25mmHg. The resulting paste is placed into a syringe and can be injected through a 6 cm long, 11-gauge needle. Following procedures similar to ASTM-F451, cylindrical samples (6 mm in diameter, 12 mm high) can be formed for compressive strength testing. The specimens are allowed to cure at atmospheric pressure (no pressure applied to curing specimens) in air at approximately 21 deg C. for 1 hour and 24 hours then subjected to compression tests. This is known as dry-testing.

#### Example Two

(0018) 35-grams mixture of 99.995% calcium sulfate hemihydrate powder manufactured as described above and placed into a bowl with about 6.65g of water and the two are mixed (water-to-powder ratio=0.19), preferably in a vacuum mixer. Preferably the calcium sulfate paste is mixed in one direction for 30 seconds at a vacuum of approximately 22-25mmHg. The resulting paste is placed into a syringe and can be injected through a 6cm long, 11-gauge needle. Following procedures similar to ASTM-F451, cylindrical samples (6mm in diameter, 12mm high) can be formed for compressive strength testing. The specimens are allowed to cure at atmospheric pressure (no pressure applied to curing specimens) in air at approximately 21 deg C. for

1 hour and 24 hours then subjected to compression tests. This is the dry-test.

### Example Three

(0019) 35-grams mixture of 99.995% calcium sulfate hemihydrate powder manufactured as described above and placed into a bowl with about 8.05 g of water and the two are mixed (water-to-powder ratio=0.23), preferably in a vacuum mixer. Preferably the calcium sulfate paste is mixed in one direction for 30 seconds at a vacuum of approximately 22-25mmHg. The resulting paste is placed into a syringe and can be injected through a 6cm long, 11-gauge needle. Following procedures similar to ASTM-F451, cylindrical samples (6mm in diameter, 12mm high) can be formed for compressive strength testing. The specimens are allowed to cure at atmospheric pressure (no pressure applied to curing specimens) in bovine serum at 37°C for 1 hour and 24 hours then subjected to compression tests. This is known as wet-testing and the results from this mode of testing are believed to be more indicative of the type of results that would result from the actual in vivo use of the material. However, the dry-testing results are correlated to wet-testing results, in the sense that the higher the compressive strength obtained in the dry-test, the higher the compressive strength that can be expected through the wet-test.



## Results

Example	Set Time	Mean Compressive Strength (MPa)	Maximum Compressive Strength (MPa)
One (dry)	1 hour	≈ 45	≈ 50
One (dry)	24 hours	≈ 88	≈ 98
Two (dry)	1 hour	≈ 49	≈ 54
Two (dry)	24 hours	≈ 98	≈ 106
Three (wet)	1 hour	≈ 49	≈ 52
Three (wet)	24 hours	≈ 56	≈ 59

(0020) After initial testing of similar samples using the same protocols, compressive strengths of 15 MPa (@ 1 hour) 35 MPa (@ 24 hours) were reported in US Provisional Patent Application Serial Number 60/444,690. The current test results exceed those early test results. As testing and mixing protocols improve, it is foreseen that the various compressive strengths produced by the invention will further increase. Accordingly, the disclosed examples are merely exemplary and not meant to be limiting.